

Prediction of oral appliance efficiency in patients with apnoea using phrenic nerve stimulation while awake

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ABSTRACT

Background In patients with sleep apnoea, primary oropharyngeal collapse of the upper airway during sleep is an important predictor of treatment success with an oral appliance. Phrenic nerve stimulation is able to induce upper airway obstruction and was therefore used to mimic the target for an efficient treatment with an oral appliance.

Objective To test if the site(s) of upper airway collapse identified by means of bilateral anterior magnetic stimulation during wakefulness could predict the efficacy of treatment with an oral appliance in patients with obstructive sleep apnoea.

Methods The site(s) of upper airway collapse while awake were identified by examining the flow–pressure relationship of flow-limited twitches when measuring velopharyngeal and oropharyngeal pressure. Once the mandibular advancement titration had been completed, the efficacy of mandibular advancement was documented during an in-lab sleep study.

Results 33 patients (24 men and 9 women, apnoea–hypopnoea index (AHI) $32.5 \pm 17.1/h$) participated in the study. Flow limitation was obtained in 29, but 3 of these had no follow-up sleep study with the device. Subjects with oropharyngeal and velopharyngeal collapse did not differ in the phenotypic characteristics associated with a positive response to an oral appliance (gender, apnoea severity, body mass index or positional dependency of breathing disturbances). Complete or partial success was seen in 14/17 subjects with twitch-induced oropharyngeal collapse and in 4/12 patients with velopharyngeal closure. Treatment response was significantly different in subjects with twitch-induced oropharyngeal and velopharyngeal collapse (OR 9.5, 95% CI 1.6 to 52.7).

Conclusions Identifying the site of upper airway collapse by using bilateral anterior magnetic stimulation of the phrenic nerve during wakefulness can predict treatment success with an oral appliance in patients with sleep apnoea.

INTRODUCTION

Obstructive sleep apnoea (OSA) is highly prevalent in modern societies and is associated with a significant increase in morbidity and mortality due to the increase in cardio-metabolic risk and vigilance impairment. Continuous positive airway pressure (CPAP) is the first recommended treatment for OSA since it is the most effective treatment for sleep-induced breathing disturbances. As it acts by pneumatic splinting of the different levels of the upper airway, the effectiveness of CPAP does not depend on the location of upper airway collapse.

However, its clinical effectiveness is limited by its cumbersome nature, and CPAP adherence is always a concern despite continuous improvements in design of the interfaces and in modalities of CPAP machine pressure delivery. For this reason, alternative therapeutic options have been developed and there is growing evidence that mandibular advancement devices (MADs) may represent an effective treatment of OSA.¹ Indeed, their ability to decrease breathing disturbance indices has been demonstrated,² in terms of improving clinical symptoms (snoring, sleep quality, excessive daytime sleepiness).^{2,3} The simplicity and ambulatory nature of treatment with MADs may account for the better adherence to MADs than to nasal CPAP.^{3,4} Unfortunately, the ability of an MAD to normalise breathing at night is not as good as for CPAP. Some anthropometric and polysomnographic parameters have been recognised as good predictors of successful MAD outcome, such as lower age, female gender, lower body mass index (BMI), lower baseline apnoea–hypopnoea index (AHI) and the presence of position dependency of sleep-disordered breathing.⁵ On the other hand, considering that an MAD prevents upper airway closure by moving the mandible and attached soft tissues forward, the site of the upper airway collapse during sleep is thought to be a powerful predictor of MAD treatment success.^{6,7} Indeed, the identification of a primary oropharyngeal obstruction during sleep has been found to be associated with a dramatic increase in success rate.⁸

Phrenic nerve stimulation, bilateral anterior magnetic phrenic stimulation (BAMPS), can reproduce during wakefulness the conditions associated with upper airway obstruction during sleep by dissociating the activity of the upper airway and inspiratory muscles.⁹ We have previously found that it may be a useful tool to identify subjects with OSA¹⁰ and to determine CPAP settings.¹¹ Moreover, this technique provides unique information on upper airway dynamic properties of the non-phasically active upper airway when the stimulus is applied during expiration and can be used to determine the site of obstruction in the upper airway by analysing the pressure–flow relationship at different pharyngeal levels.^{12,13} We hypothesised that the identification of the site of upper airway collapse when awake by means of phrenic nerve stimulation could accurately predict the efficacy of MAD treatment in patients with OSA.

The aim of our study was to assess the ability of BAMPS to identify subjects who would benefit from treatment with an MAD to improve or normalise obstructive breathing disturbances while asleep.

MATERIAL AND METHODS

Subjects

Thirty-three consecutive patients with sleep apnoea in whom mandibular advancement was retained as treatment choice participated in the study. The use of an oral appliance was proposed as a treatment using the same criteria as used in clinical practice: (1) adequate dental condition; (2) absence of any contraindication related to the temporo-mandibular joint condition; (3) mild/moderate sleep apnoea without severe daytime sleepiness that would require immediate effective treatment; or (iv) CPAP failure due to intolerance, side effects or rebutal. Other inclusion criteria included normal nose breathing, stable medical condition, no history of upper airway surgery, absence of anticipated changes in lifestyle habits (weight loss programme and medication) and absence of medication promoting weight gain or altering respiration during sleep. Sleep apnoea status was documented by a polysomnographic recording. The internal review board of our institution approved this protocol, and informed consent was obtained from every subject.

Sleep recording

Conventional polysomnographic recordings were completed according to published recommendations¹⁴ (see online repository). Sleep and respiratory variables were scored according to standard criteria.¹⁴ All electromyography (EMG), flow and pressure tracings were recorded on a microcomputer (Axoscope software 9.0; Axon Instruments, Sunnyvale, CA, USA). The baseline AHI had to be higher than 10/h for inclusion in the study.

Measurement of upper airway pressures

Silver cup electrodes were placed on the mid-clavicular line in the seventh to eighth right and left intercostal spaces for surface recording of the right and left costal diaphragmatic EMG activities (Biopac System/Biopac, Santa Barbara, California, USA). Pressure and flow recordings were completed as previously described^{10–13} (see online repository). Pharyngeal pressure was measured with a pressure-tipped catheter (model CT/S X1058, Gaeltec, Hackensack, New Jersey, USA) whose tip was positioned 2 cm below the soft palate and 4 cm down in the oropharynx (figure 1). The head position was maintained by an independent adjustable support made of two firm round pillows applied on each side of the occipital region with the head passively lying on these supports. The angle of the supports was adjusted so that the neck was strictly in alignment with the subject's back without anterior/posterior flexion. This allowed a stable and comfortable head/neck support throughout the experiment.

Phrenic nerve stimulation procedure

BAMPS was performed with two Magstim 200 stimulators (Magstim, Whitland, Dyfed, UK), connected to two 45 mm figure-of-eight-shaped coils, according to a previously described technique^{10–13 15} (see online repository). BAMPS intensity was individually set at a power output sufficient to induce clear flow-limited twitches as well as at a 20% higher intensity. As upper airway dynamic properties did not differ between the low and 20% higher stimulation intensities, only the results obtained at the low stimulation intensity will be presented.

Twitch-induced breaths were considered flow limited when instantaneous flow (\dot{V}_I) plateaued or decreased despite a persistent increase in driving pressure (P_d). A P_d versus \dot{V}_I relationship including a flow value ranging from 0 to $\dot{V}_{Im\ in}$ allowed modelling of the upper airway dynamic response of

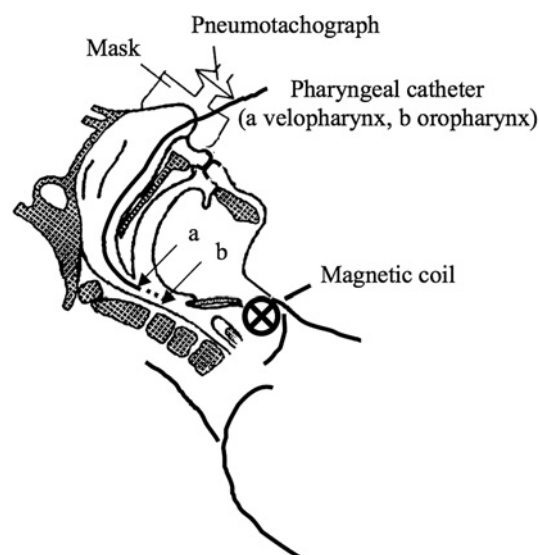


Figure 1 Schematic representation of the experimental set-up. Instantaneous flow was measured with a pneumotachograph connected to the nasal mask. Velopharyngeal and oropharyngeal pressures were recorded with a catheter positioned 2 cm below the soft palate (A) and 4 cm (B) down in the oropharynx. Phrenic nerve stimulation was performed with bilateral magnetic anterior stimulation using two figure-of-eight-shaped coils positioned anterolaterally over the anatomical landmark of the phrenic nerve in the neck.

flow-limited twitches with a polynomial regression model of the form $\dot{V}_I = k_1 P_d + k_2 P_d^2$ as previously described^{10–13} (see online repository). The flow–upper airway pressure relationships fitted well with this polynomial regression model ($r^2 \geq 0.89$, $p < 0.001$). The site(s) of upper airway collapse induced by BAMPS was identified by examining the flow–pressure curves and the k_1/k_2 ratio at the velopharyngeal and oropharyngeal levels. Criteria used to detect the presence of oropharyngeal or velopharyngeal collapse were defined a priori. Exclusive oropharyngeal collapse was identified by the presence of flow limitation exclusively when the catheter was in the distal position (figure 2). In the presence of velopharyngeal collapse, flow limitation was observed at both the upper and lower pressure measurements sites (figure 2). The presence of exclusive velopharyngeal collapse was identified by the occurrence of flow limitation with the catheter below the soft palate and a difference between the k_1/k_2 ratio measured at the oropharyngeal and velopharyngeal levels ≤ 0 cm H₂O. Primary oropharyngeal collapse was identified when this difference was >1 cm H₂O. This threshold was chosen according to the reproducibility of twitch-by-twitch closing pressure values obtained in our laboratory and of the variability in velopharyngeal closing pressure values during sleep.⁸

MAD titration procedure

This was completed by one of the investigators (JFM) after identification of the collapsing site with the phrenic nerve stimulation technique. The choice of the device (ORM, ResMed, San Diego, California, USA; TAP or Silent Nite, Glidewell Laboratories, Newport Beach, California, USA) was made by this investigator according to his clinical experience. Following an initial acclimatisation period, the MAD was progressively advanced to obtain an optimal response based on the assessment of subjective (symptoms resolution, abolition of snoring, improvement in daytime sleepiness according to the Epworth

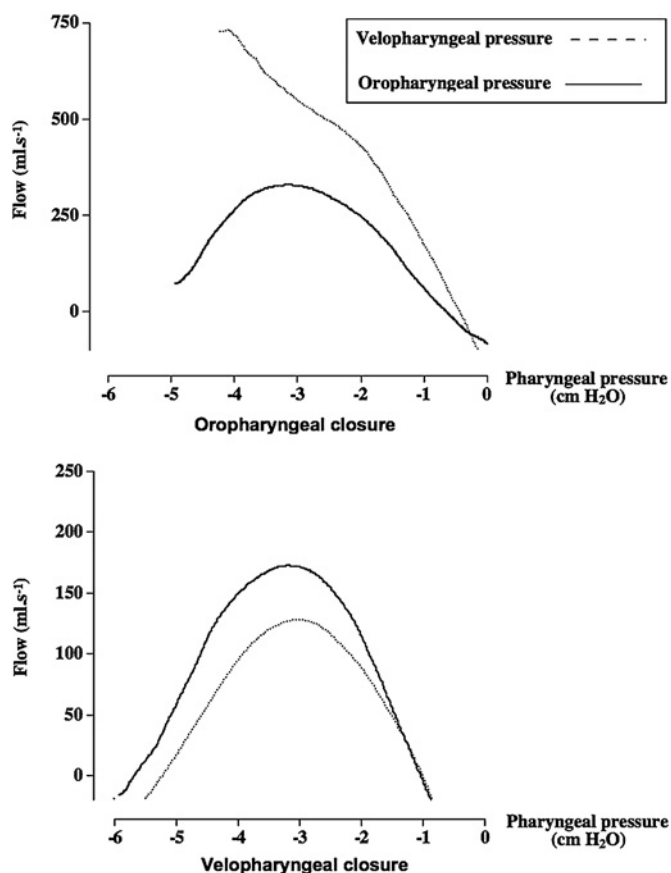


Figure 2 Representative examples of flow–pressure tracings obtained in two subjects demonstrating oropharyngeal and velopharyngeal closure, respectively. Oropharyngeal closure is characterised by the dissociation between twitch flow and oropharyngeal pressure tracings with no plateauing in velopharyngeal pressure. In the case of velopharyngeal closure, the flow–pressure tracings obtained at each site are closely parallel and dissociated from flow tracing.

Sleepiness Score (ESS)) and objective (abbreviated home respiratory recording: Apnoea link, version 6.0, ResMed, Poway, California, USA)¹⁶ variables or until maximal tolerance.

Study design

Phrenic nerve stimulation was applied with the catheter positioned at the velopharyngeal or oropharyngeal level and at the two stimulation intensities in random order. Subjects were not instructed regarding the time when the twitch was to be applied. Five twitches were delivered in each condition and two recording sessions were obtained at each upper airway level. The site of upper airway collapse was determined by analysis of the flow–pressure curves (see below). Patients were referred to the dentist for completion of MAD titration following completion of the phrenic nerve stimulation measurements. After the dentist had determined the optimal amount of mandibular advancement, the efficacy of the MAD was documented by an in-lab sleep study. Subjects were asked to quantify their perceived improvements in snoring, sleep quality and energy on a Likert scale. The dentist and technicians who scored the sleep recording were blind to the results of the BAMPs procedure.

Outcome measures

Treatment response was evaluated following the control polysomnographic study completed with the MAD in an intention

to treat approach. Subjects with an AHI <10/h were classified as responders and those with an AHI ≥10 but with a >50% reduction in AHI as partial responders. Treatment failure was defined as the absence of clinical benefit, loss on follow-up and/or <50% reduction in AHI when compared with baseline.

We determined that 21 subjects should be included if 90% of patients who will improve and 20% of those who will not improve with an MAD would be identified with phrenic nerve stimulation with a responder/non-responder ratio of 2:1 and a 80% power at a 0.05 significance level. This number was increased to 33 taking into consideration a 25% procedure failure rate and a 25% drop-out rate.

Analysis

Qualitative data are presented as percentages and quantitative data as mean±SD or median (min–max). Differences in proportions were tested with the χ^2 test or the Fisher exact test, and continuous variables were compared with the Student t test or the Wilcoxon test according to the distribution of the data. The normality assumption was verified with the Shapiro–Wilk test, and the Brown and Forsythe variation of the Levene test statistic was used to verify the homogeneity of variances. Univariate and multivariate logistic regressions were performed to predict the success of the oral appliance in the presence of oropharyngeal closure. Continuous variables were checked for the assumption of linearity in the logit, and the graphical representations suggested linear relationships. The Hosmer–Lemeshow test was performed to assess the goodness-of-fit of the models. The results were considered significant with p values <0.05. The data were analysed using the statistical package program SAS v9.2.

RESULTS

Anthropometric characteristics of participating patients are reported in table 1. An MAD represented the first-line treatment in 28 subjects while it was indicated due to CPAP intolerance in the other five. The site of upper airway collapse with phrenic nerve stimulation could not be determined in four subjects (intolerance of the procedure in one subject, absence of pressure recording due to technical problems in one and small driving pressure and absence of a flow-limited twitch in the two others). Two other subjects stopped treatment before having completed the MAD home titration procedure (absence of treatment benefits in one and side effects (excessive salivation) in the other) and one further subject was lost on follow-up. These

Table 1 Characteristics of subjects who completed or did not complete the study

	Study completed (n = 26)	Study not completed (n = 7)	p Value
Age (years)	51±11	52±10	0.79
Gender (males/females)	18/8	6/1	0.64
Baseline BMI (kg/m ²)	27.8±4.3	27.9±4.2	0.92
Baseline AHI (n/h)	30.3±18.5	29.7±11.4	0.63
Baseline AHI <30 n/h (%)	46.1	71.4	0.46
SDB position dependency (%)	28.0	28.6	1.0
Velopharyngeal/oropharyngeal closure (n)	10/16	2/1	0.53
Success rate (%)	69.2	42.9	0.19

In the group who did not complete the study, the site of upper airway collapse was determined in three subjects who did not undergo a control study with their MAD, and the success rate was established in the four subjects who had no flow-limited twitches but had a control study. Values are given as the mean±SD.

AHI, apnoea–hypopnoea index; BMI, body mass index; SDB, sleep-disordered breathing.

Table 2 Values of closing pressure measured at the velopharyngeal and oropharyngeal level depending on the main site of twitch-induced upper airway collapse

	k_1/k_2	
	Velopharynx	Oropharynx
Exclusive velopharyngeal closure (n=12)	-8.5±2.8	
Exclusive oropharyngeal closure (n=9)		-7.5±2.8
Primary oropharyngeal closure (n=8)	-8.9±2.4	-7.3±2.6

three subjects were considered as treatment failures. Therefore, complete results could be obtained in 26 subjects. From these, 11 were treated with an ORM, 11 with a TAP and 4 with a Silent Nite device. Subjects who completed the study can be considered as representative of the whole group since there was no difference in the characteristics of subjects who completed or did not complete the study (table 1). In subjects who did not complete the study, 4 were treated with an ORM and 3 with a TAP. It is noteworthy that all but one subject who had no follow-up study with a MAD had exclusive velopharyngeal closure.

Effective BAMPS intensity ranged from 40% to 100% (74±19% max). The site of upper airway collapse was remarkably reproducible between the two recording sessions obtained at the velopharyngeal and oropharyngeal sites (difference in the k_1/k_2 ratio for a given upper airway site=0.3±0.7 cm H₂O). Twitch-induced flow limitation occurred exclusively at the velopharyngeal site in 12 subjects, at the oropharyngeal site in 9 others (exclusive oropharyngeal collapse) and in the 8 others the oropharyngeal segment was found to be more collapsible (less negative closing pressure) than the velopharyngeal site (primary oropharyngeal collapse) (table 2).

An MAD was associated with an improvement in AHI, supine AHI, sleep fragmentation, nocturnal desaturation and diurnal somnolence (ESS) with no change in BMI (table 3). Improvement in sleep fragmentation and in subjective assessment of sleep quality and energy were greater in subjects with treatment success than in those with no improvement in breathing disorders (data not shown). Complete or partial success was seen in 14/17 subjects with twitch-induced oropharyngeal collapse and in 4/12 patients with velopharyngeal closure (table 4). Treatment response was significantly different in subjects with twitch-induced oropharyngeal and velopharyngeal collapse (sensitivity 82.4, 95% CI 58.9% to 93.8%; specificity 66.7%, 95% CI 39.1% to 86.2%; OR 9.5, 95% CI 1.6 to 52.7, p=0.02). This provided a positive likelihood ratio of 2.5 and, given the overall

Table 3 Baseline and control values of sleep and respiratory variables in the 26 patients who completed the study

	Baseline	With an MAD	p Value
Age (years)	51±11		
Gender (males/females)	18/8		
BMI (kg/m ²)	27.8±4.3	27.6±4.4	0.33
AHI (n/h)	30.3±16.9	10.9±8.8	<0.01
Supine AHI (n/h)	51.8±19.1	19.6±12.6	<0.01
Time supine (% TST)	44.7±24.4	45.7±23.8	0.81
ESS	10.8±4.9	6.4±3.3	<0.01
Sleep efficiency (%)	75.3±15.3	82.8±9	0.02
% TST <90% SaO ₂	0.2 (0.0–7.8)	0.0 (0.0–2.1)	<0.01
Respiratory arousal index (n/h)	13.5 (6.0–60.8)	5.3 (0.4–38.0)	<0.01

Except for % TST <90% SaO₂ and the respiratory arousal index that are expressed as median (min–max), variables are reported as the mean±SD.
AHI, apnoea–hypopnoea index; BMI, body mass index; ESS, Epworth Sleepiness Score.

Table 4 Characteristics of patients demonstrating velopharyngeal or oropharyngeal (exclusive or primary) collapsing sites according to BAMPS

	Site of obstruction		p Value
	Velopharynx	Oropharynx	
Complete responder (n=14)	3	11	0.03
Partial responder (n=4)	1	3	
Failure (n=11)	8	3	
Age (years)	51±10	50±12	0.81
Gender (male/female)	10/2	10/7	0.23
Neck circumference (cm)	38.7±3.2	37.7±3.1	0.39
Baseline BMI (kg/m ²)	27.1±2.4	28.1±5.1	0.51
Baseline AHI (n/h)	33.9±21.9	27.9±10.9	0.40
Baseline AHI <30 n/h (%)	58.3	41.2	0.46
SDB position dependency (%)	33.3	23.5	0.38
Skeletal class I (n)	6	6	0.86
Skeletal class II (n)	5	9	
Skeletal class III (n)	1	2	

AHI, apnoea–hypopnoea index; BAMPS, bilateral anterior magnetic phrenic stimulation; BMI, body mass index; SDB, sleep-disordered breathing.

63.6% success rate of MADs, the likelihood of treatment success associated with oropharyngeal collapse increased to 81.4%. On the other hand, given the negative likelihood ratio of 0.26 associated with velopharyngeal closure, the likelihood of treatment failure decreased from 36.4% to 12.9%. Skeletal class data were available in all but one subject who demonstrated oropharyngeal closure. Skeletal class, neck circumference, pharyngeal grade or mallampati score did not differ significantly between subjects with velopharyngeal or oropharyngeal collapse (p=0.86) (table 4). Interestingly, subjects with oropharyngeal and velopharyngeal collapse did not differ in the phenotypic characteristics that have been reported to be helpful in the identification of good responders to MAD treatment (gender, apnoea severity, BMI, positional dependency of breathing disturbances) (table 4). Univariate analysis demonstrated no association between these parameters and MAD response at a p value of 0.2, indicating that none of these parameters improved the predictive value associated with the identification of the pharyngeal site.

DISCUSSION

Our results demonstrate that the identification of upper airway collapse during wakefulness using phrenic nerve stimulation is a useful tool to identify patients with sleep apnoea who are good candidates for treatment with an MAD.

Without considering BAMPS results on identification of the collapsing site, the overall success rate of MADs was 69.2%. This appears to be higher than the 52% average ability of an MAD to decrease the AHI below 10/h⁵ but is close to that recently reported in other studies.¹⁷ Such a high success rate can also be accounted for by the use of an abbreviated sleep recording to optimise MAD titration.¹⁶ The better success rate previously observed by Fleury *et al* using this strategy (complete response in 63.6% and partial response in 18.2%) may relate to the difference in the population studied. In our patients, no further adjustment of the MAD could be done in patients with treatment failure. It should be stressed that the proposed phrenic stimulation technique provided relevant measures on upper airway collapse characteristics in the majority of the subjects (30/33), technical failure being observed in only four patients (12%). This 9% rate is one-third of the discontinuation rate reported in one of the

largest studies that evaluated conditions associated with success of oral appliances in OSA.⁵

The criteria used to define treatment success correspond to those currently used the most in the literature.¹ This choice is clinically relevant when comparing the present results with previously reported treatment success rates. We considered that a definition of treatment success based on an AHI <5/h with an MAD was not relevant with the scoring criteria that were used. These were retained because in these subjects with clinical features of sleep apnoea, breathing abnormalities were not consistently associated with a 4% SaO₂ fall but more often with sleep fragmentation. Considering the improvement in sleep quality and diurnal somnolence that we observed and the beneficial effects of MAD treatment on arterial pressure and oxidative stress and on endothelial dysfunction reported with AHI values on MAD at 12±2/h¹⁸ and 19.6±11.5/h, respectively,¹⁹ we are confident of the efficacy of the treatment as assessed in our study.

Nasal CPAP and MADs both have their respective advantages and disadvantages. When a guaranty of effectiveness is concerned, CPAP is to be considered as the reference treatment. It also allows patients to have a treatment trial without having to purchase the apparatus. On the other hand, when considering the issue of compliance, this has been found to be higher with a MAD than with CPAP. However, the cost of treatment with a MAD can influence treatment choice since nocturnal breathing disturbances can persist in ~50% of patients.¹ This justifies the need to identify phenotypes prone to predict the response to an MAD, and results from large follow-up studies previously demonstrated that gender, weight, baseline AHI and the supine dependence of breathing disturbances may help to predict treatment response.

Strategies aimed at better identification of responders/non-responders have also been developed taking into account that advancement of the mandible affects the upper and lower upper airway segments differently. Mandibular advancement induces a larger improvement in oropharyngeal than in velopharyngeal cross-sectional area in both anaesthetised obese and non-obese subjects.²⁰ This is in accordance with the dramatic influence of the site of upper airway collapse measured during sleep on MAD treatment success. Henke *et al* found that the decrease in AHI was greater in subjects who had upper airway closure below the velopharynx compared with those who had velopharyngeal collapse.⁶ Improvement in oropharyngeal patency with mandibular advancement has also been documented by sleep nasoendoscopy in patients whose AHI improved with an MAD.²¹ Using a multisensor pressure transducer to identify the site of upper airway collapse during sleep, Ng *et al* demonstrated that 100% of subjects with oropharyngeal obstruction normalised their AHI with a MAD while only 37.5% of patients with velopharyngeal closure were cured.⁸ Therefore, identifying the site of upper airway collapse during sleep provides unique information on future MAD treatment response in patients with OSA. However, the need for investigations of upper airway mechanics during sleep reduces the practical applicability of these techniques.

This led to the evaluation of the discriminative nature of tests performed during wakefulness. MRI of the pharynx during tidal breathing and the Müller manoeuvre demonstrate that the pattern of upper airway obstruction without and with an MAD reflects the response to treatment with an MAD.⁷ In a retrospective analysis, Otsuka *et al* found that airway space, and oropharyngeal airway cross-sectional area were larger and the position of the mandible relative to the cervical spine was longer

in subjects who did not improve with an MAD.²² A pilot study performed with functional imaging recently suggested that upper airway modelling may be used to predict outcomes of treatment with MADs, the increase in upper airway volume being correlated with improvement in apnoea severity with MADs.²³ Finally, the Müller manoeuvre performed during nasopharyngoscopy with mandibular advancement identified that airway collapse was greater in the velopharynx in non-responders than in responders and was still observed with an MAD.²⁴ It should be emphasised that the above-mentioned studies compared upper airway static or dynamic features that would discriminate MAD responders and non-responders, but the predictive value of the proposed models has not been prospectively validated. In fact, prospective evaluation of procedures such as analysis of features of the inspiratory and expiratory flow–volume curves was not found to be helpful to discriminate between responders and non-responders to MADs.²⁵ The effects of an MAD on the upper airway mechanical properties assessed have been previously reported in normal subjects, demonstrating a decrease in the propensity for the upper airway to collapse with an MAD.²⁶

The results of the recent study of Chan *et al*²⁷ are interesting to discuss in parallel with the present results. These authors found no difference in MRI-assessed volume of airway or soft tissue structures between responders and non-responders to an MAD. However, a significant enlargement of the upper airway volume was observed with an MAD in responders mainly due to an increase in the volume and lateral dimension of the velopharynx. Thus the success of an MAD could be influenced by its ability to stabilise pharyngeal structures at the velopharyngeal level. In our study, 8/16 subjects with primary oropharyngeal collapse also demonstrated velopharyngeal closure at lower upper airway pressures. In these subjects, the velopharyngeal closing pressure (as assessed by the k_1/k_2 ratio) did not differ from that measured in patients with primary velopharyngeal closure (table 2). On the other hand, independently of the primary closure level, the velopharyngeal closing pressure was less negative in non-responders (−8.5±1.8 cm H₂O) than in responders (−9.5±2.5 cm H₂O). However, this difference did not reach significance. Thus, additional experiments aimed at quantifying the effect of mandibular advancement on velopharyngeal collapsibility and its influence on the response to an MAD would be worth completing. In this instance, the identification of the upper airway obstruction site with a phrenic nerve stimulation technique while awake inscribes into a clinical investigation strategy where knowledge transfer should result in important applications in sleep apnoea treatment strategies.

We conclude that the identification of the anticipated response to an MAD by means of phrenic nerve stimulation during wakefulness represents an important clinical step in the management of sleep apnoea. According to the present data, the predictive value of BAMPs-derived identification of the site of upper airway occlusion is higher than that using conventional characterisation of phenotypic patients. Since it does not require patients to buy any device, such a procedure could be very effective in targeting subjects who would or would not benefit from MAD treatment and could be integrated into the investigation strategy of candidate subjects.

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Competing interests None.

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Correction

D S Stavroulias, K L Lau, I O Oey, *et al.* Thoracoscopic bullectomy for dyspnoea in emphysema: defining new boundaries. *Thorax* 2010;**65**:A137. The authors names appeared incorrectly in this abstract. The names should have appeared as follows: D Stavroulias, K Lau, I Oey, A Nakas, S Rathinam, D A Waller.

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Material and methods

Sleep recording

Conventional polysomnographic recordings were completed according to published recommendations [12]. They consisted of in-lab continuous acquisition of electroencephalogram, electrooculogram, submental electromyogram, arterial oxyhemoglobin saturation by transcutaneous pulse oxymetry, naso-oral airflow with thermistor, nasal pressure with nasal canula, chest and abdominal movements by impedance plethysmography (RespiraceTM, Ambulatory Monitoring Inc., Ardsley, NY), electrocardiogram, and breath sounds. Sleep position was continuously assessed by the attending technician with an infrared camera. All variables were digitally recorded (Sandman EliteTM System, Mallinckrodt, Kenilworth, NJ).

Measurement of UA pressures

Silver cup electrodes were placed on the mid-clavicular line in the seven to eight right and left intercostal spaces for surface recording of the right and left costal diaphragmatic EMG activities (Biopac System/Biopac, Santa Barbara, CA). Pressure and flow recordings were completed as previously described [8-11]. After local anesthesia (xylocaine 2 % spray) of one nostril, a pressure-tipped catheter (model CT/S X1058, Gaeltec, Hackensack, NJ) was passed through one nostril and its position was marked when its tip was 2 cm below the soft palate and 4 cm down in the oropharynx (figure 1). A plastic nasal stent was placed in the anterior nares to prevent nasal collapse. A continuous positive airway pressure nasal mask was then placed over the nose with the catheter passing through one drilled hole. Occlusion of the mask opening during maximal

inspiratory efforts was used to assess its airtightness. A second catheter was passed through another opening of the mask to measure pressure inside the mask. A pneumotachograph (model 112467-3850A, Hans Rudolf, Kansas City, MO) connected to the mask was used to obtain instantaneous flow. Pressures and flow were digitally recorded at 2000 Hz sample rate (Digidata 1320, Axon Instrument, Foster City, CA). Subjects were seated in a comfortable armchair with a 60 degree inclination. Measurements were obtained during exclusive nasal breathing.

Phrenic nerve stimulation procedure

BAMPS was performed with two Magstim 200 stimulators (Magstim, Whitland, Dyfed, UK), connected to two 90° handle 45-mm eight-shaped coils, according to previously described technique [8 – 11, 13]. Each stimulating coil was positioned anterolaterally over the anatomical landmark of the phrenic nerve in the neck by a high precision multipositional support consisting of two articulated arms (MAN 143; Manfrotto Trading, Bassano del Grappa, Italy) (figure 1). The optimal position and orientation of the coils was determined separately for each side. The two stimulators were triggered by a timer driven by the changes in flow direction, the 1 ms twitches being delivered 2 seconds after expiratory onset. BAMPS intensity was individually set at a power output sufficient to induce clear flow-limited twitches as well as at a 20 % higher intensity.

Analysis

Sleep and respiratory variables were scored according to standard criteria [12]. All EMG, flow and pressure tracings were recorded on a microcomputer (Axoscope software 9.0;

Axon Instruments). Twitch-induced breaths were considered flow-limited when instantaneous flow (\dot{V}_I) plateaued or decreased despite a persistent increase in driving pressure (P_d). A P_d versus \dot{V}_I relationship including flow value ranging from 0 to \dot{V}_{Imin} allowed to model the UA dynamic response of flow-limited twitches with a polynomial regression model of the form $\dot{V}_I = k_1 P_d + k_2 P_d^2$ as previously described [8 -11]. Solving the last equation for $\dot{V}_I = 0$ results in $P_d = -k_1/k_2$ and provides a value of the driving pressure at which the UA will be closed. As a consequence, the k_1/k_2 ratio describes UA closing pressure (the less negative the k_1/k_2 , the higher the UA collapsibility). Polynomial model fitting and determinations of k_1 and k_2 values were performed semi-automatically using custom-made software (JMP 7.0; SAS Institute, Cary, NC).