Non-invasive assessment of pulmonary blood flow using an inert gas rebreathing device in fibrotic lung disease

Tamera J Corte, ¹ Athol U Wells, ¹ Michael A Gatzoulis, ¹ Derek Cramer, ¹ Simon Ward, ¹ Peter S Macdonald, ² Konstantinos Dimopoulos, ¹ Stephen J Wort ¹

¹Royal Brompton Hospital and National Heart and Lung Institute, London, UK ²University of New South Wales, Sydney, Australia

Correspondence to

Dr Stephen John Wort, Pulmonary Hypertension Unit, Royal Brompton Hospital, Sydney St, London SW3 6NP, UK; s.wort@imperial.ac.uk

Received 5 June 2009 Accepted 30 January 2010

ABSTRACT

Background and aims Pulmonary hypertension (PH) is increasingly recognised in patients with diffuse lung disease, and is associated with increased mortality. Cardiac output (CO) is a prognostic marker in PH. Non-invasive assessment of pulmonary blood flow (PBF_{INNOCOR}) with the inert gas rebreathing Innocor device has been validated against CO in PH, but not in PH associated with parenchymal lung disease. PBF_{INNOCOR} may be less accurate in patients with lung disease because of intrapulmonary shunting and/or incomplete gas mixing. Our aim was to determine the variability of PBF_{INNOCOR} in normal subjects, before evaluating PBF_{INNOCOR} in diffuse lung disease against CO measured by the indirect Fick method (CO_{FICK}) at right heart catheterisation (RHC).

Methods and results 23 normal subjects had lung volume measurements by a constant-volume body plethysmograph and three consecutive PBF_{INNOCOR} measurements on the same day. 20 subjects returned for repeat assessment. PBF_{INNOCOR} had good intrasession repeatability (coefficient of variation (CV)=6.57%) and intersession reproducibility (mean CO difference=0.13; single determinant SD=0.49; CV=9.7%). 28 consecutive patients with lung fibrosis referred for RHC had PBF_{INNOCOR} measured within 24 h of RHC. There was good agreement between CO_{FICK} and PBF_{INNOCOR}, with no evidence of systematic bias (mean CO_{FICK} 4.3 \pm 1.0; PBF_{INNOCOR} 4.0 \pm 1.2l/ min; p=0.07). Bland—Altman analysis revealed a mean difference of -0.32 and limits of agreement of -2.10 to +1.45.

Conclusion Non-invasive PBF measured by the inert gas rebreathing Innocor device has good intrasession repeatability and intersession reproducibility. In diffuse lung disease, CO can be accurately and non-invasively measured by the Innocor device.

INTRODUCTION

Pulmonary vascular limitation is increasingly recognised as a major complication of diffuse fibrotic lung disease. In idiopathic pulmonary fibrosis (IPF) the reported prevalence of pulmonary hypertension (PH) ranges from 31% to 85%. ^{1–6} PH is associated with clinical deterioration and higher mortality in patients with IPE. ^{3 7 8} Currently, the diagnosis of PH rests on haemodynamic parameters measured on right heart catheterisation (RHC), as non-invasive markers such as echocardiography are less reliable in diffuse lung disease. ^{9–11} Reproducible, reliable non-invasive prognostic markers are thus highly desirable in this high-risk patient group.

Cardiac output (CO) is an important prognostic marker in pulmonary arterial hypertension (PAH)^{12 13} although its role in parenchymal lung disease has not been specifically studied. Traditional assessment of CO is by RHC, using thermodilution or the direct or indirect Fick method. However, RHC is invasive, and not always practicable in the context of diffuse lung disease. The non-invasive assessment of CO by the foreign gas rebreathing method is well established and validated against more invasive CO measurements.¹⁴ The foreign gas rebreathing method involves the inhalation of a gas mixture containing a soluble and an insoluble gas. The pulmonary blood flow (PBF) is proportional to the rate of decline of the soluble compound, and is considered equivalent to CO in the absence of cardiopulmonary shunting. Historically, the respiratory mass spectrometer has been used for such measurements, but these instruments are bulky, difficult to operate and costly to maintain. However, the more recently developed Innocor machine, which uses the inert gas rebreathing technique with continuous photoacoustic gas analysis, is less expensive, portable and easier to use. Non-invasive PBF assessment with the Innocor has been validated against CO measured at RHC in patients with heart failure¹⁵ and PAH, ¹⁶ but not in PH associated with parenchymal lung disease. Inert gas rebreathing measures of CO may be less accurate in patients with diffuse lung disease because of intrapulmonary shunting and/or incomplete gas mixing.

In this study, in order to examine its utility in patients with diffuse lung disease, we first determine the intrasession repeatability and intersession reproducibility of the Innocor PBF measurement in normal subjects. Secondly, we examine the Innocor measurement of PBF against invasive CO assessment (by the indirect Fick method) in patients with diffuse fibrotic lung disease.

METHODS

Subjects

Normal subjects

Ethical approval was obtained from the local ethics committee for this study. Twenty-three subjects (eight male; mean age 34 ± 8 years) without underlying lung disease were recruited via in-hospital advertisement, and informed consent was obtained. Lung volumes were measured by a constant-volume body plethysmograph. On the same day, subjects underwent three consecutive PBF measurements with the Innocor device. Twenty-one (91%)

Interstitial lung disease

subjects returned on a separate day for repeat CO measurements (1-13 weeks later).

Subjects with fibrotic lung disease

Twenty-eight consecutive patients with fibrotic lung disease (16 males, mean age $63\pm12\,\mathrm{years}$) undergoing RHC for assessment for PH were recruited, and informed consent was obtained. RHC was performed when there was clinical suspicion of PH based on echocardiographic and pulmonary function parameters, and right heart overload and/or failure on examination. All patients underwent pulmonary function testing prior to RHC.

Non-invasive PBF assessment with the Innocor device was performed within 24 h of RHC by trained personnel, blinded to the RHC results. Three consecutive non-invasive PBF measurements were obtained and the mean value calculated (PBF $_{\rm INNOCOR}$).

Measurements

Non-invasive PBF assessment

Subjects, sitting upright at rest, breathed through a closedcircuit system (Innocor, Innovision, Denmark). This rebreathing system uses an inert soluble gas (0.5% nitrous oxide) and an inert insoluble gas (0.1% sulfur hexafluoride) and 28% oxygen in N₂ in a 2–4 litre rubber bag. The volume to which the bag was filled was adjusted to 60% of the subjects' vital capacity. Rebreathing was performed over a 30 s period, and subjects followed a graphical tachometer on the computer screen and verbal prompts to ensure a respiratory rate of 20 breaths/min. Subjects were instructed to empty the rebreathing bag completely with each breath, to ensure a constant ventilation volume. Gas was sampled continuously from the mouthpiece, and rapid photoacoustic spectroscopic analysers measured gas concentrations. The PBF was calculated from the rate of uptake of nitrous oxide into the blood. In subjects without pulmonary arterial-venous shunting, PBF_{INNOCOR} is considered equal to CO.

Right heart catheterisation

RHC measurements were performed at rest in the supine position, using standard techniques (Swan-Ganz catheters, Edwards Life Sciences, Irvine, California, USA) and the following pressure measurements were performed: systolic, diastolic and mean pulmonary artery pressure (mPAP); and systolic, diastolic and mean right atrial pressure. Left heart catheterisation was also performed in order to measure systemic arterial pressure, left atrial pressure and left ventricular end-diastolic pressure (LVEDP).

CO was calculated using Fick's principle, with oxygen consumption estimated using standardised reference tables 17 according to the following equation 18 19 :

CO_{FICK} = oxygen uptake/

(arterial oxygen concentration—venous oxygen concentration)

CO was adjusted for body surface area to cardiac index. 20 Pulmonary vascular resistance (PVR) was calculated according to the formula 21 :

PVR = (mPAP-mLAP)/CO

LVEDP was used to estimate mean left atrial pressure (mLAP). Pulmonary capillary wedge pressure was not determined due to the potential increased risk of pulmonary arterial rupture

and/or haemorrhage in patients with abnormal pulmonary vasculature. 22

Pulmonary function testing

Predicted pulmonary function values were calculated using a European Community for Coal and Steel publication. The American Thoracic Society (ATS)/European Respiratory Society (ERS) guidelines were followed when the lung function tests were performed. Lung volumes (constant-volume body plethysmograph), spirometric volumes and single-breath diffusion capacity of the lung for carbon monoxide (DLCO) were measured (Jaeger Masterscreen; Cardinal Health UK 240, Warwick, UK). End capillary (ear-lobe) blood gas analysis was performed on room air (n=21; 348 Blood Gas Analyser; Siemens Healthcare Diagnostics, Sunbury, UK).

Statistical analysis

All analyses were performed using STATA statistical software (version 10.0; StataCorp, College Station, Texas, USA). Data are expressed as the mean and SD or median and range, as appropriate. A p value of <0.05 was considered statistically significant.

Normal subjects

The intrasession repeatability of the $PBF_{INNOCOR}$ measurement was determined by the coefficient of variation (CV) calculated by the following equation: $CV=100\times(SD)/mean$. Intersession reproducibility of the $PBF_{INNOCOR}$ was assessed by Bland—Altman analysis, with single determinant SD, and CV.

Subjects with pulmonary fibrosis

The relationship between invasive (CO_{FICK}) and non-invasive ($PBF_{INNOCOR}$) measures of CO was examined using Bland—Altman analysis. Results are expressed as mean CO difference (bias), limits of agreement (\pm 2 SD).²⁷

RESULTS

Normal subjects

The clinical characteristics of the normal subjects are shown in table 1. Twenty-one subjects were life-long non-smokers, and two were ex-smokers. One had a history of mild asthma, but was taking no regular medication. All subjects had lung volumes within the predicted normal range.

Baseline parameters as assessed by the Innocor device are displayed in table 1 including a mean PBF $_{\rm INNOCOR}$ of 5.27 ± 1.14 l/min, and a mean SD of 0.32 ± 0.20 l/min. There was good intrasession repeatability, with a CV of 6.34%. The intersession reproducibility was high, with a mean PBF difference of 0.12 and a single determinant SD of 0.49. The intersession CV was 9.29%.

Subjects with pulmonary fibrosis

Baseline parameters

The baseline characteristics of the 28 patients are summarised in table 2. Patients had fibrotic lung disease, including IPF (n=15), non-specific interstitial pneumonia (n=10) and chronic hypersensitivity pneumonia (n=2). Sixteen (52%) were life-long non-smokers, with 12 (43%) ex-smokers (mean 18 pack-years). One patient had a history of atrial fibrillation, and eight had systemic hypertension, with the remaining 18 patients having no significant cardiac history. Most patients were functionally impaired, in WHO functional class III (n=13) or IV (n=12). Eight (26%) were in right heart failure.

Table 1 Baseline characteristics of normal subjects (n=23)

(II LO)	
Characteristics*	
Age (years)	34±8
Gender	8 male; 15 female
Height	170±9 cm
Weight	73±21 kg
Pulmonary function tests:	
Total lung capacity (%)	$101 \pm 14\%$
Functional residual capacity (%)	$105 \pm 17\%$
Vital capacity (%)	102±15%
Baseline Innocor parameters:	
Heart rate	$77 \pm 9 \text{bpm}$
Residual volume (V _L)	$2.96 \pm 0.40 \text{litres}$
Pulse oximetry	$98\!\pm\!2\%$
Pulmonary blood flow (cardiac output)	5.27 ± 1.14 l/min
Cardiac index	2.90 ± 0.53 l/min/m ²
Stroke volume	$69.68\!\pm\!19.13\text{ml}$

^{*}Mean±SD.

Baseline mean gas transfer was $23.4\pm7.4\%$, forced vital capacity $61.5\pm29.6\%$, and Pao_2 $7.98\pm1.9\,kPa$. Twenty of 28 (71%) had PH on RHC: mPAP $28.5\pm9.4\,mm$ Hg; LVEDP $9.1\pm4.0\,mm$ Hg, PVR 4.7 ± 3.0 Wood's units and CO_{FICK} $4.3\pm1.0\,l/min$. With the Innocor device, mean PBF $_{INNOCOR}$ was $4.0\pm1.2\,l/min$.

Relationship between invasive and non-invasive CO measurements. There was good agreement between CO year and PRE process.

There was good agreement between CO_{FICK} and $PBF_{INNOCOR}$ (figure 1), with no evidence of systematic bias, as judged by

Table 2 Baseline characteristics of subjects with pulmonary fibrosis (n=28)

Characteristics*	
Age (years)	63±12
Height	168 ± 9 cm
Weight	78±16 kg
Pulmonary function tests	
Total lung capacity (%)	$61.4 \pm 21.0\%$
DL _{CO} (%)	$23.4 \!\pm\! 7.4\%$
K _{CO} (%)	$49.3\!\pm\!14.1\%$
FEV ₁ (%)	$60.7 \pm 18.2\%$
FVC (%)	$61.5\!\pm\!19.6\%$
Pao ₂ (n=21)	$8.0\pm1.9\text{kPa}$
Right heart catheter	
mPAP	28.5 ± 9.4 mm Hg
mRAP	$5.1\pm3.0\text{mm}$ Hg
LVEDP	$9.1\pm4.0\mathrm{mm}$ Hg
Cardiac output	$4.3 \pm 1.0 \text{ l/min}$
Cardiac index	$2.3\!\pm\!0.5\text{l/min/m}^2$
Pulmonary vascular resistance	$4.7 \pm 3.0 WU$
Baseline Innocor parameters:	
Heart rate	84±14 bpm
Residual volume	2.0 ± 0.5 litres
Pulse oximetry	$91.3 \pm 4.8\%$
Pulmonary blood flow (cardiac output)	4.0 ± 1.2 l/min
Cardiac index	$2.1\pm0.6l/min/m^2$
Stroke volume	$47.8 \pm 17.1 ml$

^{*}Mean±SD.

DL_{CO}, diffusion capacity for carbon monoxide; FEV₁, forced expiratory volume in 1 s; FVC, forced vital capacity; K_{CO}, diffusion capacity corrected for alveolar volume; LVEDP, left ventricular end-diastolic pressure; mPAP, mean pulmonary artery pressure; mRAP, mean right atrial pressure; Pao₂, arterial partial pressure for oxygen; WU, Wood's units.

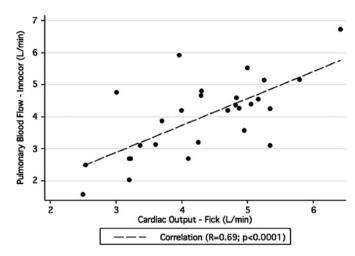


Figure 1 Correlation of cardiac output measured by right heart catheter and pulmonary blood flow measured by the inert gas rebreathing technique (Pearson correlation).

Student paired t test: mean CO_{FICK} 4.3±1.0, mean $PBF_{INNOCOR}$ 4.0±1.2 l/min (p=0.07). Bland—Altman analysis revealed a mean difference of -0.32 (95% CI -0.67 to 0.02) with limits of agreement of -2.10 to +1.45 l/min (figure 2).

DISCUSSION

In this study we demonstrate that PBF as measured on the Innocor device is both repeatable and reproducible in normal control subjects. The intrasession CV of 6.3% and intersession CV of 9.3% are similar to those for other pulmonary physiological parameters, and within acceptable limits. Secondly, we assess the accuracy of the non-invasive PBF $_{\rm INNOCOR}$ against the invasive CO $_{\rm FICK}$ measurement in patients with interstitial lung disease. We demonstrate good agreement between these measurements.

Pulmonary vascular limitation and PH are important complications of diffuse lung disease. PH is associated with increased mortality in diffuse lung disease. In the search for reliable prognostic markers, a number of pulmonary vascular parameters have been studied. On RHC, elevated mPAP is

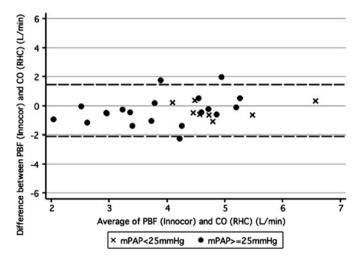


Figure 2 Bland—Altman plot for cardiac output (CO) measured by right heart catheter (RHC) and pulmonary blood flow (PBF) measured by the inert gas rebreathing technique (Innocor). mPAP, mean pulmonary artery pressure.

associated with increased mortality in IPF,^{3 8} and elevated PVR is related to higher mortality in advanced lung disease.²⁸ Reduced CO has been established as an important poor prognostic marker in PAH,^{12 13} but this has not been specifically studied in diffuse lung disease. While it is current practice to perform an RHC in the assessment of PH in patients with lung fibrosis, RHC is not always practicable in these patients. Furthermore, repeat RHC for monitoring disease progression and response to treatment is clearly undesirable in this patient population. For this reason, a reliable, reproducible, non-invasive prognostic marker is desirable for this patient group.

Foreign gas rebreathing methods non-invasively estimate PBF. PBF is calculated using a rebreathing manoeuvre whereby the patient breathes a mixture containing a soluble and an insoluble gas. By continuous sampling of the gas concentrations, the rate of reduction of the soluble gas can be calculated. This rate is proportional to the PBF, and CO in the absence of a significant shunt. Respiratory mass spectrometers use the foreign gas rebreathing method, and are safe and reliable in the estimation of PBF and CO.14 There is good correlation between CO measured on mass spectrometry and the direct Fick method in healthy subjects, PAH and severe heart failure.^{29 30} Limited data for the clinical utility of mass spectrometers are available outside the intensive care setting. Gatzoulis et al demonstrated an increase in PBF in Eisenmenger patients following bosentan treatment, and suggested that it may be a useful clinical tool in monitoring of PAH. $^{31~32}$ In practice, however, respiratory mass spectrometers are bulky, costly and require regular calibration and maintenance, making their widespread clinical use difficult.

More recently, the foreign gas rebreathing method has been incorporated with photoacoustic spectroscopy analysis in the Innocor device. Photoacoustic spectroscopy uses pulsatile exposure of the measured gases to filtered light, creating pressure oscillations. Measurement of these oscillations by a microphone provides an indirect measurement of gas concentrations. This device is simple to use, mobile and less costly than the traditional respiratory mass spectrometer. PBF_INNOCOR correlates with CO_FICK better than CO as measured by thermodilution. ³³ PBF_INNOCOR has been validated against CO_FICK in heart failure at rest and on exercise, ¹⁵ $^{33-35}$ and PAH (published in abstract form). ¹⁶

However, no studies have specifically focused on patients with diffuse lung disease. There are potential limitations for this device in the context of parenchymal lung disease. 36 First, parenchymal lung disease may inhibit complete alveolar gas mixing (which is an essential assumption for the calculation of CO by this method). Secondly, intrapulmonary shunting of blood through areas of poor gas exchange will not be measured by this method, therefore potentially underestimating the total PBF in these patients. However, these potential problems are not supported by the results of the current study in which a good agreement between PBF_INNOCOR and CO_FICK is demonstrated.

The results of this study are limited by the fact that the PBF_{INNOCOR} and CO_{FICK} measurements were not performed simultaneously. CO is a relatively labile measurement, varying with body position and time of day. Despite the potential variability in CO, we showed good agreement between the two measurements when performed within 24 h of each other. However, the lability of CO may partly explain the imperfect agreement between the two measurements.

The results of the current study are necessarily limited by selection bias, by recruiting patients referred for RHC. To minimise selection bias, a simple, inclusive, prospective approach was undertaken in which consecutive patients with

interstitial lung disease referred for RHC were recruited. As a result, the present study includes patients with a variety of histological diagnoses, including two patients with hypersensitivity pneumonitis. It is possible that patients with hypersensitivity pneumonitis may have increased intrapulmonary shunting related to local areas of consolidation. However, this is unlikely, as our results remained significant with the exclusion of these two patients (results not shown). We also have a high proportion of patients with PH (71%), and patients on supplemental oxygen (81%) in our cohort. It is possible that results may differ for patients with milder disease. However, patient numbers in this study are relatively small, and do not allow analysis of subgroups according to the presence of PH, or oxygen requirements. The results of this study cannot be generalised to the interstitial population at large.

In this study, the oxygen consumption necessary for calculating CO by the Fick principle was estimated from normograms rather than directly measured. While measurement of oxygen consumption is desirable, it can be cumbersome and prone to technical errors in non-intubated patients relating to inadequate timing or collection of samples, continuous oxygen administration and abnormal breathing patterns due to anxiety, sedation or pulmonary disease. Still, estimation of CO by the Fick principle is more reliable than thermodilution methods, especially in patients with low CO. As most adult catheterisation laboratories nowadays use assumed VO₂ values, our study was designed to compare the Innocor with standard catheter laboratory practice. Further studies are needed comparing Innocor measurement and Fick calculation with assumed VO₂ values with the gold standard of Fick with direct VO₂ measurement.

On the basis of the current study, PBF measurement with the Innocor is a repeatable, reproducible, easily performed technique. Although we demonstrate good agreement between PBF INNOCOR and COFICK, PBF INNOCOR is unlikely to replace CO_{FICK} as other important markers such as pulmonary arterial pressures are also measured at RHC. However, PBF INNOCOR is a potential prognostic marker for patients with diffuse lung disease, and may be useful in follow-up in monitoring for disease progression and response to advanced treatment. Clearly, the widespread clinical application of this technique in the evaluation of patients with diffuse lung disease and possible PH remains to be determined. A larger study inclusive of patients with varied disease severity, and with clinical follow-up is warranted to establish its prognostic value.

CONCLUSION

Non-invasive PBF as measured by the inert gas rebreathing Innocor device has good intrasession repeatability and intersession reproducibility. In patients with diffuse fibrotic lung disease, CO may be accurately and non-invasively measured by the Innocor inert gas rebreathing device. Further longer term studies are required to determine the potential clinical and prognostic role of this non-invasive CO measurement.

Funding Actelion Pharmaceuticals-Educational Grant.

Competing interests None.

Ethics approval This study was conducted with the approval of the Brompton, Harefield and NHLI Research Ethics Committee.

Provenance and peer review Not commissioned; externally peer reviewed.

REFERENCES

 Shorr AF, Wainright JL, Cors CS, et al. Pulmonary hypertension in patients with pulmonary fibrosis awaiting lung transplant. Eur Respir J 2007;30:715—21.

- Nadrous HF, Pellikka PA, Krowka MJ, et al. The impact of pulmonary hypertension on survival in patients with idiopathic pulmonary fibrosis. Chest 2005;128(6 Suppl):616S—17S.
- Lettieri CJ, Nathan SD, Barnett SD, et al. Prevalence and outcomes of pulmonary arterial hypertension in advanced idiopathic pulmonary fibrosis. Chest 2006;199:746—52
- Yang SJ, Hoffman C, Mulligan K, et al. Pulmonary arterial hypertension in patients with idiopathic pulmonary fibrosis when listed for lung transplantation and at lung transplantation. Proc Am Thorac Soc 2006;3:A369.
- Agarwal R, Gupta D, Verma JS, et al. Noninvasive estimation of clinically asymptomatic pulmonary hypertension in idiopathic pulmonary fibrosis. Indian J Chest Dis Allied Sci 2005;47:267—71.
- Nathan SAS, Koch J, Barnett S, et al. Serial measures of pulmonary artery pressures in patients with idiopathic pulmonary fibrosis. Chest 2005;128:168S.
- Nadrous HF, Pellikka PA, Krowka MJ, et al. Pulmonary hypertension in patients with idiopathic pulmonary fibrosis. Chest 2005;128:2393—9.
- Hamada K, Nagai S, Tanaka S, et al. Significance of pulmonary arterial pressure and diffusion capacity of the lung as prognosticator in patients with idiopathic pulmonary fibrosis. Chest 2007;131:650—6.
- Homma A, Anzueto A, Peters JI, et al. Pulmonary artery systolic pressures estimated by echocardiogram vs cardiac catheterization in patients awaiting lung transplantation. J Heart Lung Transplant 2001;20:833—9.
- Ben-Dor I, Kramer MR, Raccah A, et al. Echocardiography versus right-sided heart catheterization among lung transplantation candidates. Ann Thorac Surg 2006:81:1056—60.
- Arcasoy SM, Christie JD, Ferrari VA, et al. Echocardiographic assessment of pulmonary hypertension in patients with advanced lung disease. Am J Respir Crit Care Med 2003;167:735—40.
- D'Alonzo GE, Barst RJ, Ayres SM, et al. Survival in patients with primary pulmonary hypertension. Results from a national prospective registry. Ann Intern Med 1991:115:343—9
- Sandoval J, Bauerle O, Palomar A, et al. Survival in primary pulmonary hypertension. Validation of a prognostic equation. Circulation 1994;89:1733—44.
- Sackner MA, Greeneltch D, Heiman MS, et al. Diffusing capacity, membrane diffusing capacity, capillary blood volume, pulmonary tissue volume, and cardiac output measured by a rebreathing technique. Am Rev Respir Dis 1975;111:157—65.
- Agostoni P, Cattadori G, Apostolo A, et al. Noninvasive measurement of cardiac output during exercise by inert gas rebreathing technique: a new tool for heart failure evaluation. J Am Coll Cardiol 2005;46:1779—81.
- Mclure L, Brown A, Peacock A, et al. Non-invasive assessment of pulmonary blood flow using an inert gas rebreathing device in patients with pulmonary hypertension. Thorax 2007;62 SIII. (abstract S33).
- Cholley BP, Payen D. Noninvasive techniques for measurements of cardiac output. Curr Opin Crit Care 2005;11:424—9.
- Ultman JS, Bursztein S. Analysis of error in the determination of respiratory gas exchange at varying FIO2. J Appl Physiol 1981;50:210—16.

- Mathews L, Singh RK. Cardiac output monitoring. Ann Card Anaesth 2008:11:56—68.
- Du Bois D, Du Bois EF. A formula to estimate the approximate surface area if height and weight be known. 1916. *Nutrition* 1989;5:303—11; discussion 312—13
- Mazza E, Taichman D. Functions and control of the pulmonary circulation. In: Mandel J. Taichman D, eds. *Pulmonary vascular disease*. Philadelphia: Elsevier, 2006: 1—19.
- Mullerworth MH, Angelopoulos P, Couyant MA, et al. Recognition and management of catheter-induced pulmonary artery rupture. Ann Thorac Surg 1998;66:1242—5.
- 23. **Gibson GJ.** Standardised lung function testing. *Eur Respir J* 1993:**6**(Suppl):1—100.
- Wanger J, Clausen JL, Coates A, et al. Standardisation of the measurement of lung volumes. Eur Respir J 2005;26:511—22.
- Macintyre N, Crapo RO, Viegi G, et al. Standardisation of the single-breath determination of carbon monoxide uptake in the lung. Eur Respir J 2005;26:720—35.
- Miller MR, Hankinson J, Brusasco V, et al. Standardisation of spirometry. Eur Respir. J. 2005; 26:319—38
- Critchley LA, Critchley JA. A meta-analysis of studies using bias and precision statistics to compare cardiac output measurement techniques. J Clin Monit Comput 1999;15:85—91.
- Selimovic N, Andersson B, Bergh CH, et al. Pulmonary hemodynamics as predictors of mortality in patients awaiting lung transplantation. Transpl Int 2008;21:314—19.
- Hoeper MM, Maier R, Tongers J, et al. Determination of cardiac output by the Fick method, thermodilution, and acetylene rebreathing in pulmonary hypertension. Am J Respir Crit Care Med 1999;160:535—41.
- Kallay MC, Hyde RW, Smith RJ, et al. Cardiac output by rebreathing in patients with cardiopulmonary diseases. J Appl Physiol 1987;63:201—10.
- Gatzoulis MA, Rogers P, Li W, et al. Safety and tolerability of bosentan in adults with Eisenmenger physiology. Int J Cardiol 2005;98:147—51.
- Gatzoulis MA, Barst B, Fineman J, et al. Eisenmenger syndrome and pulmonary arterial hypertension in adults with congenital heart disease. Curr Med Res Opin 2007;23:S19—25.
- Gabrielsen A, Videbaek R, Schou M, et al. Non-invasive measurement of cardiac output in heart failure patients using a new foreign gas rebreathing technique. Clin Sci (Lond) 2002:102:247—52.
- Dong L, Wang JA, Jiang CY. Validation of the use of foreign gas rebreathing method for non-invasive determination of cardiac output in heart disease patients. J Zhejjiang Univ Sci 2005;6:1157—62.
- Lang CC, Karlin P, Haythe J, et al. Ease of noninvasive measurement of cardiac output coupled with peak VO2 determination at rest and during exercise in patients with heart failure. Am J Cardiol 2007;99:404—5.
- Friedman M, Wilkins SA Jr, Rothfeld AF, et al. Effect of ventilation and perfusion imbalance on inert gas rebreathing variables. J Appl Physiol 1984:56:364—9.
- Morten D, Peter N. Effects of ventilation on cardiac output determined by inert gas rebreathing. Clin Physiol Funct Imaging 2005;25:142—7.